



# Ultrasonic Strain Image Made by Speckle Tracking of B-mode Image

---

學生: 呂仁碩 李承諺 葉文俊

指導教授: 李百祺

# Introduction

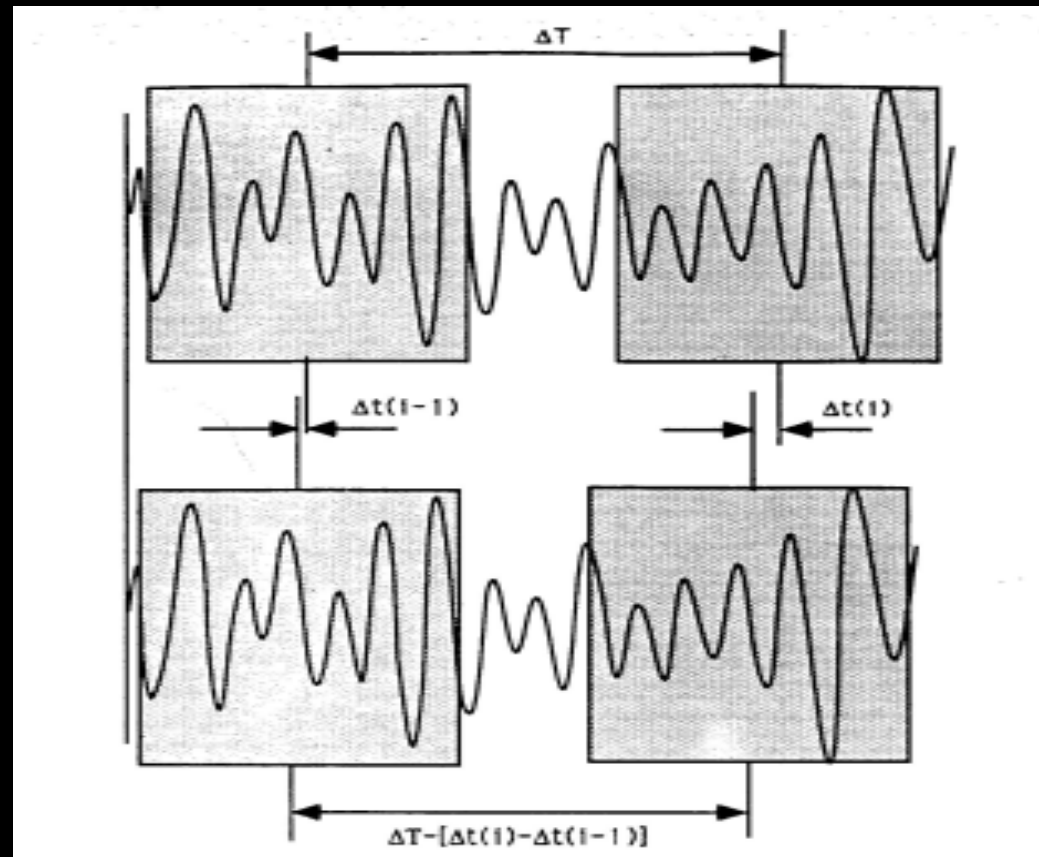
---

- Elasticity imaging can provide a significant adjunct to current diagnostic ultrasonic methods
- Most elasticity imaging is derived by RF data and few by envelope data.
- RF data elasticity imaging is more sensitive; envelope data is less noisy under larger strain

# Strain estimation by RF data

Cross correlation of consequent A-line

$$s(i) = \frac{\Delta t(i) - \Delta t(i-1)}{\Delta T}$$



# Strain estimation by envelope data

## --Speckle tracking of B-mode image

---

- 1D-cross correlation of consequent column of pixels (like A-line of RF data)(Ophir) : lateral displacement is hard to detect.
- 2D-Block matching algorithm (Levinston, 1994; Yeung, 1997), time costing full search and multi-level methods

# Goal of this project

---

- studying the differences of 1D and 2D methods
- studying the differences of full search and multilevel speckle tracking method
- searching other possible strain estimator

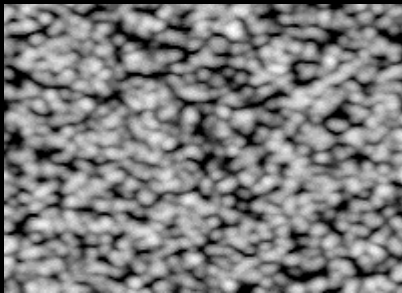
# Materials and Methods

---

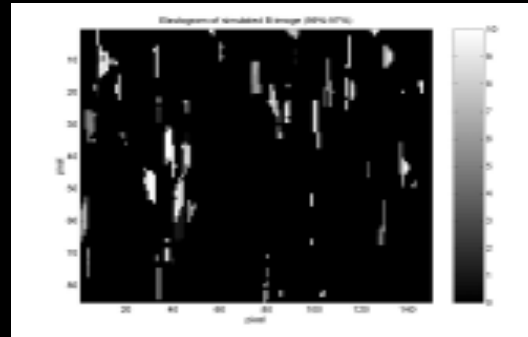
- Target: B-mode images
  - simulated data set
  - breast phantom
  - clinical breast tumor
- Method: 1D and 2D speckle tracking

# Result-I

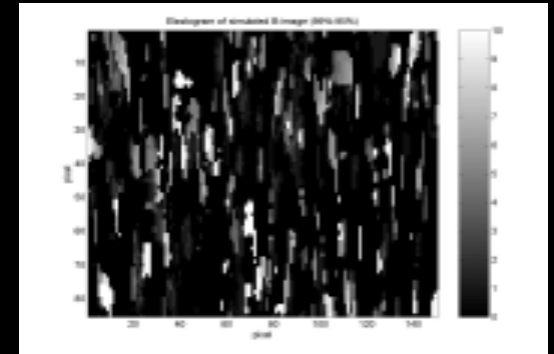
- Comparison of Elastogram1 (1D and 2 D)



1D

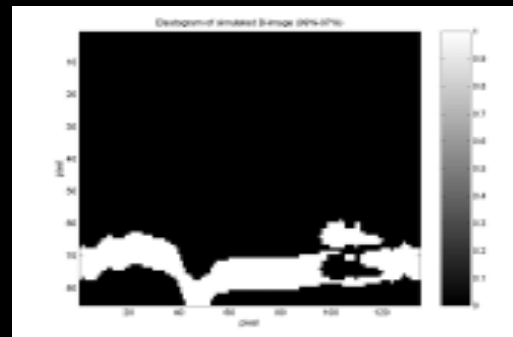


99-97%

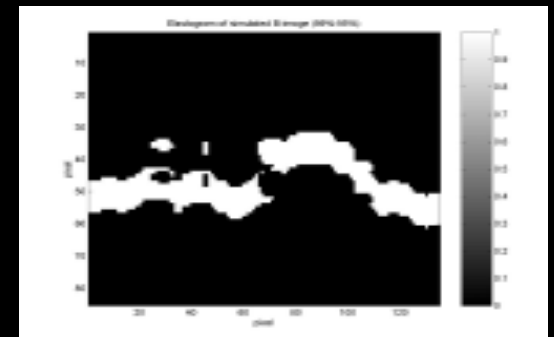


99-95%

2D



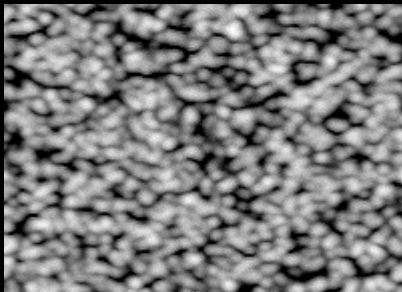
99-97%



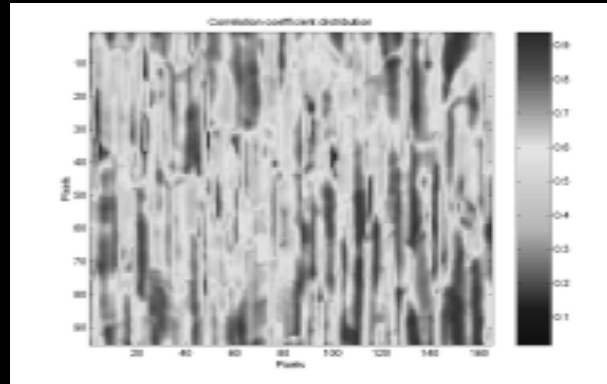
99-95%

# Result-1

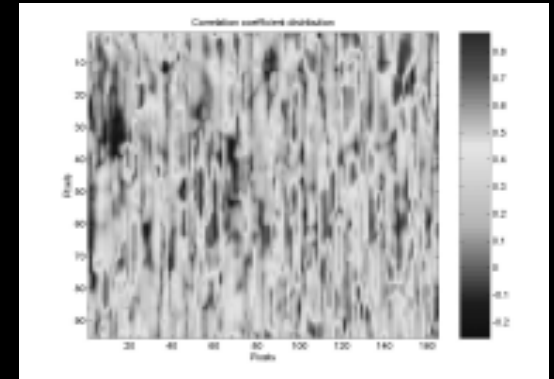
- Comparison of correlation coefficients distribution (1D and 2 D)



1D

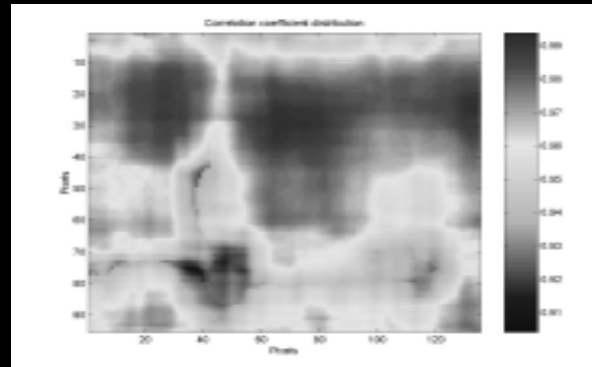


99-97%

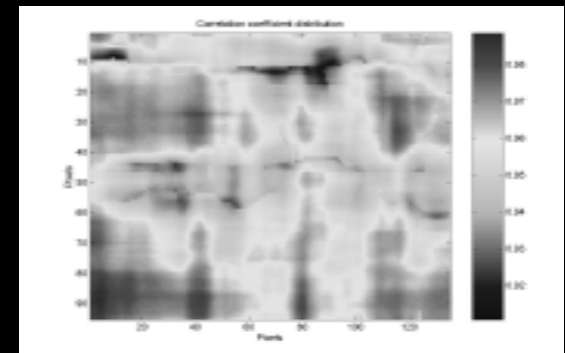


99-95%

2D



99-97%

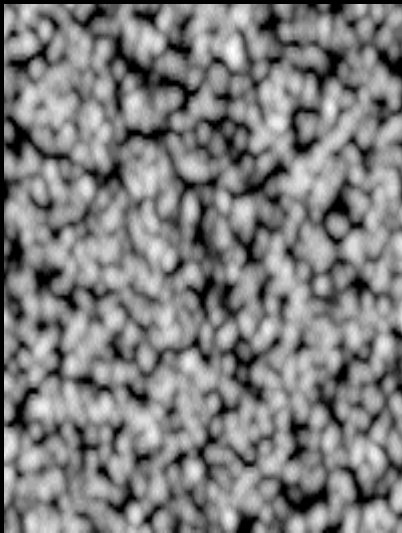


99-95%

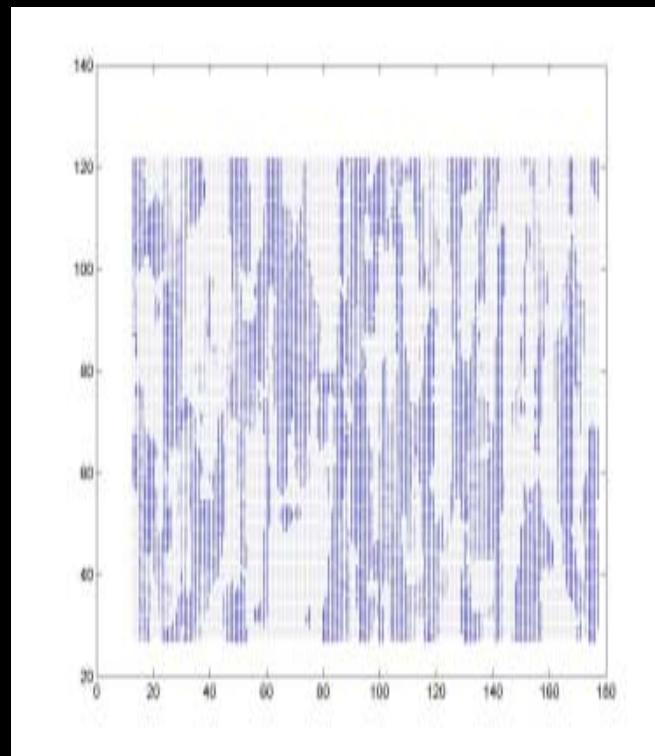


# Result-I

- Comparison of arrow direction distribution (1D and 2 D)

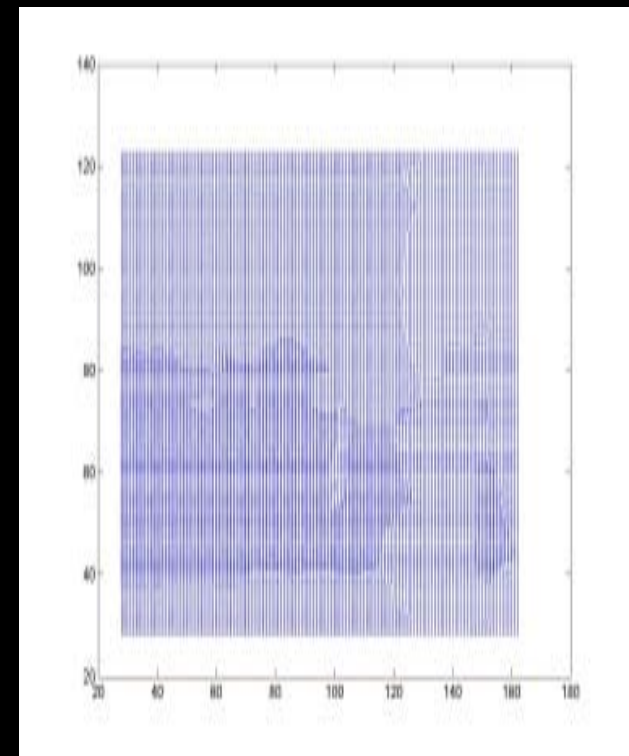


1D



99-95%

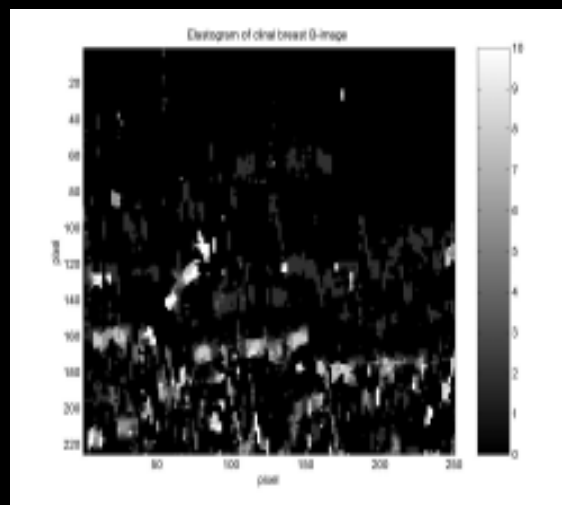
2D



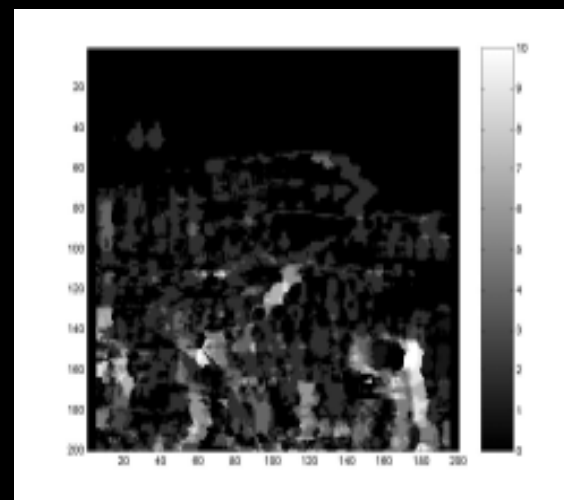
99-95%

# Result-I

---



1D



2D

# Improved Speckle Tracking - Multi-level

- Multiple levels, 9 points estimation in each level

Image Before  
In-plane Motion

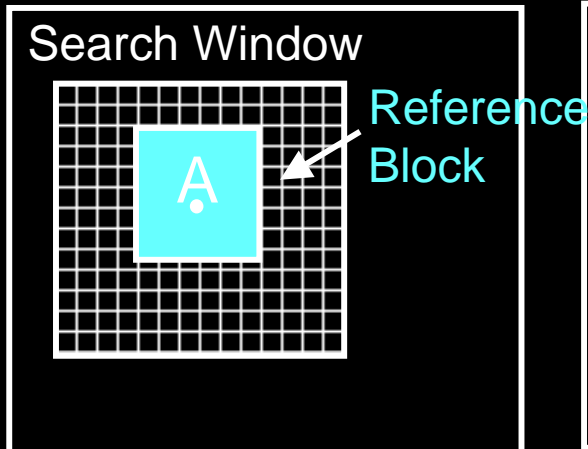
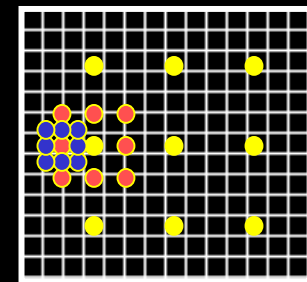
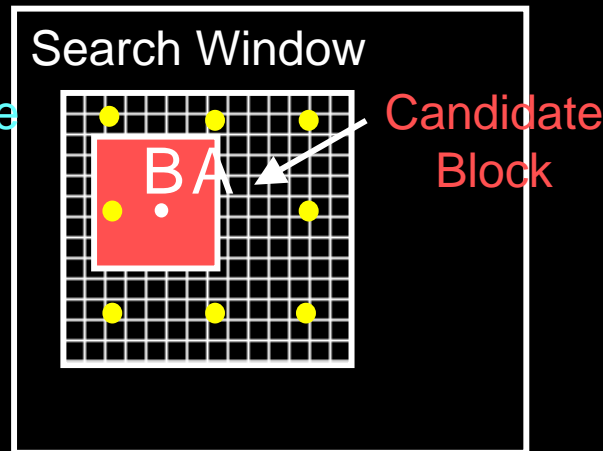
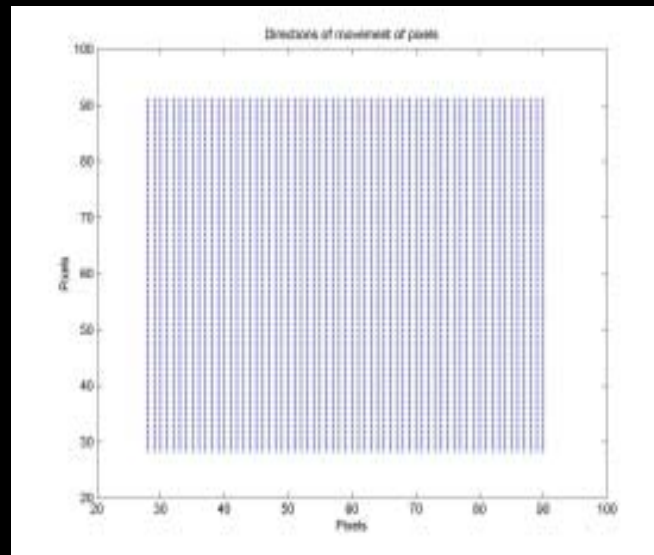


Image After  
In-plane Motion

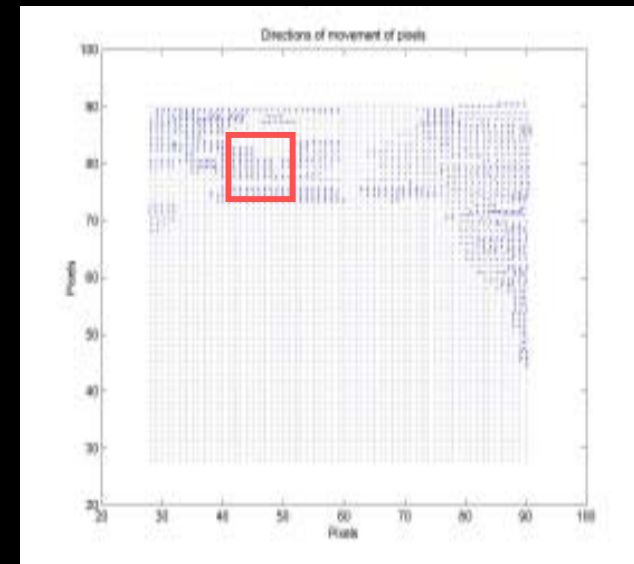


# Result-II

- Comparison of full search and mult-level speckle tracking method

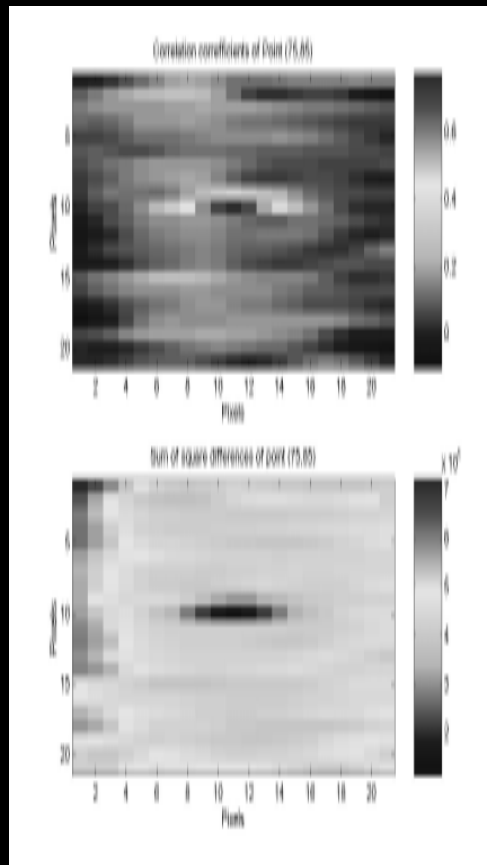


Full search



Two level

# Result-II



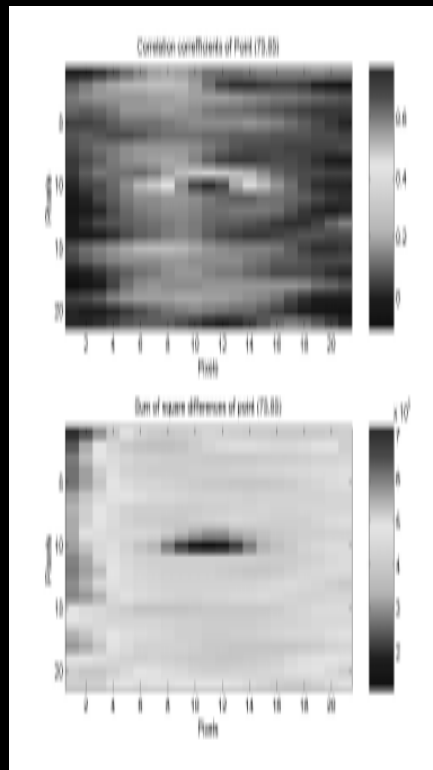
D1

475311	427026	456354
	(111365)	
479950	421806	423350
500169	405354	405057

C1

0.1438	0.1397	0.0552
	(0.7736)	
0.1021	0.1378	0.0935
0.0486	0.1856	0.1605

# Result-II



D2		
451723	426930	457179
	(111516)	
451620	427890	424554
482545	413751	411719
C2		
0.1463	0.1166	0.0326
	(0.7655)	
0.1353	0.0969	0.0751
0.0804	0.1434	0.1265

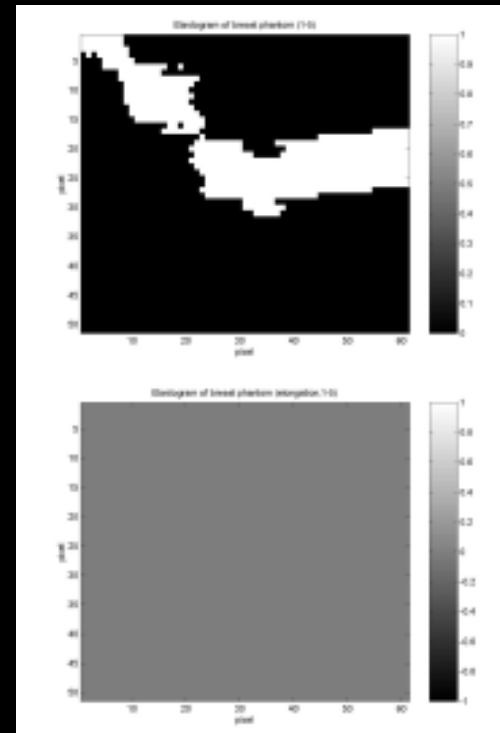
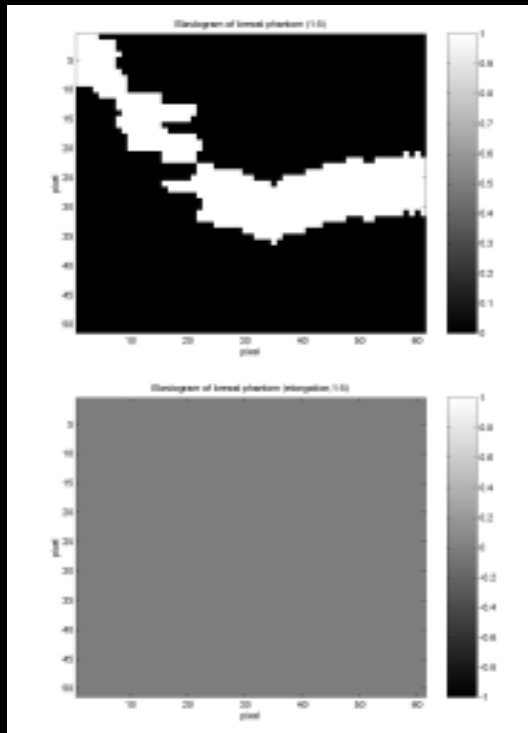
# Result-II

- Comparison of full search method of sum of difference and correlation coefficient

Sum of difference (1-5)

Correlation coefficient

Vertical strain

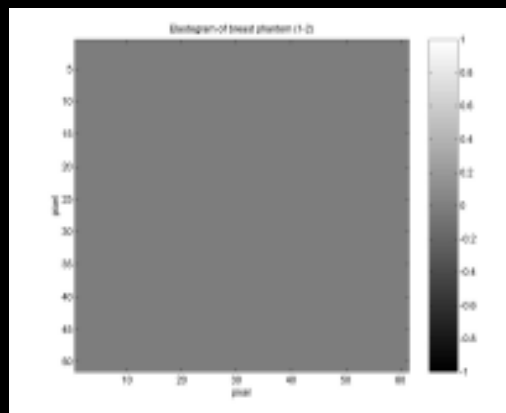


Elongation

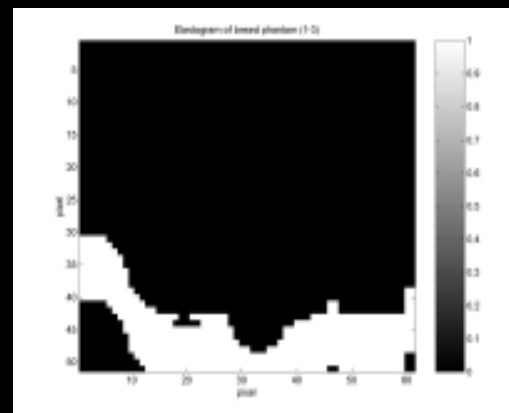
# Result-II

	Sum of differences		Correlation coefficients	
	Minimal cc	Mean cc	Minimal cc	Mean cc
1-2	0.7387	0.8962	0.7387	0.8962
1-4	0.3944	0.7810	0.3944	0.7810
1-5	0.3520	0.7677	0.3520	0.7679

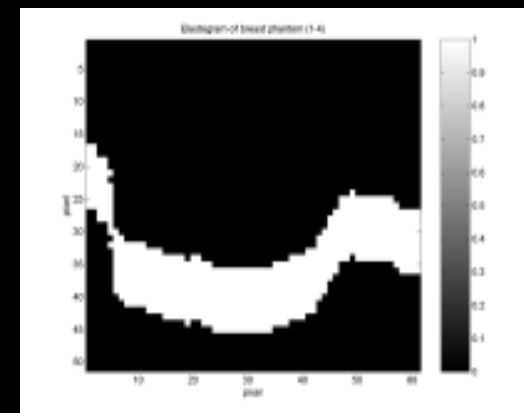
1-2



1-3



1-4

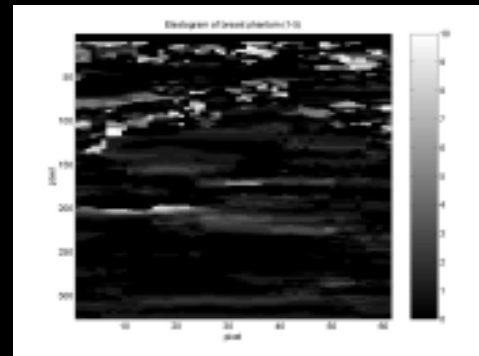
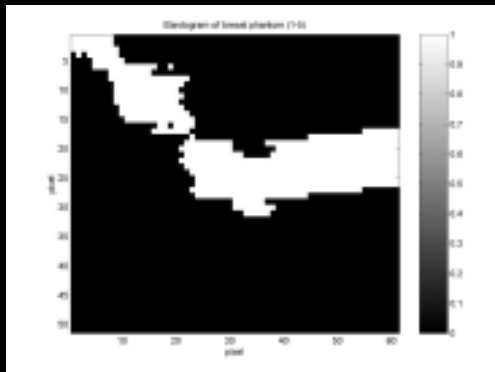




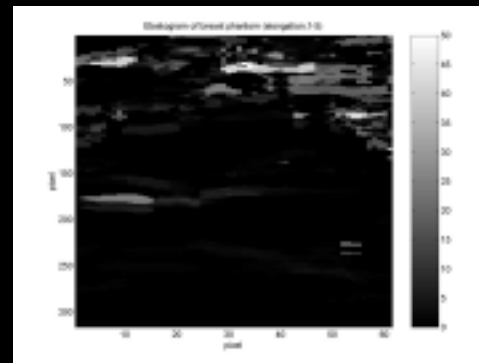
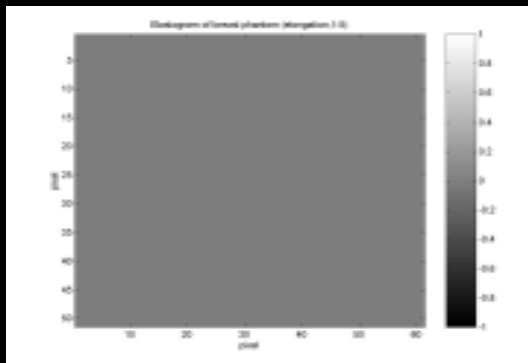
# Result-II

- Interpolation (1 pixel --> 5 pixels)

Vertical strain

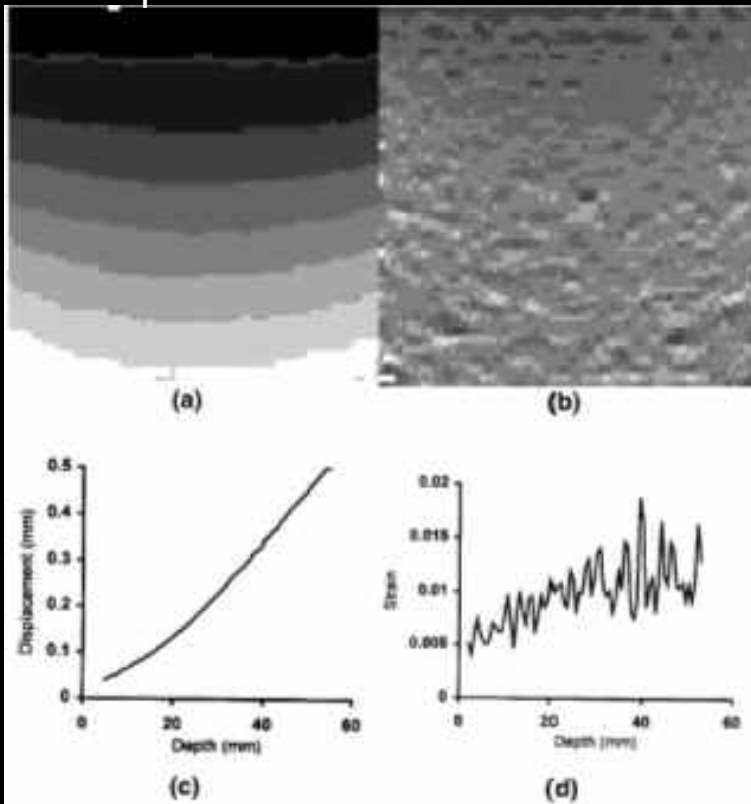


Elongation

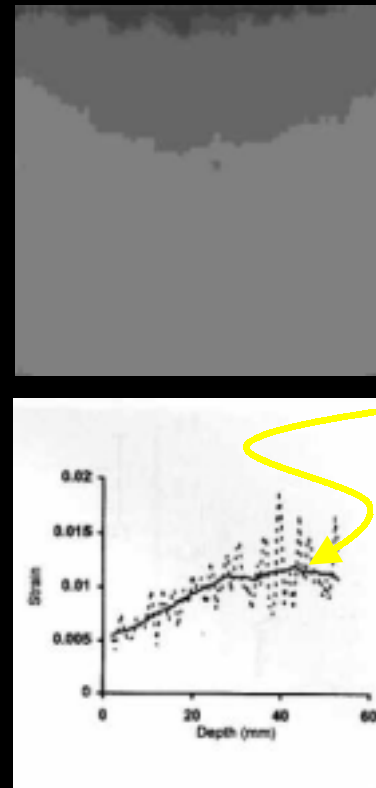


# LSQSE (Least Square Strain Estimator)

Homogeneous Strain Image obtained by  
gel phantom taking the gradient  
From 1% applied of the displacement field  
compression



After LSQSE



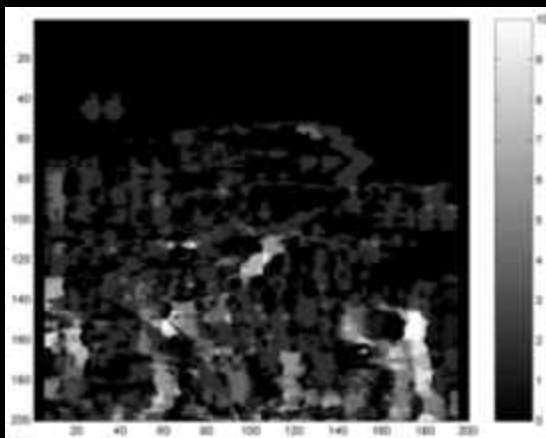
The middle column from the LSQ strain image

# LSQSE (Least Square Strain Estimator)

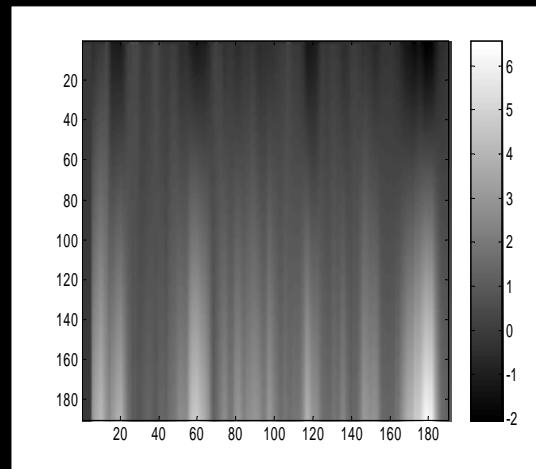
Origin Image



Full Search SAD Result

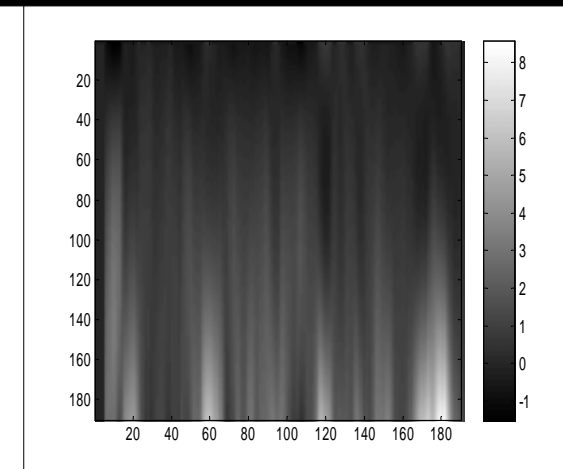


LSQ order 1



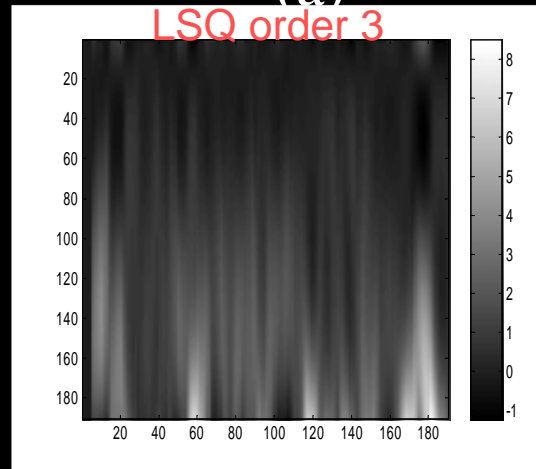
(a)

LSQ order 2



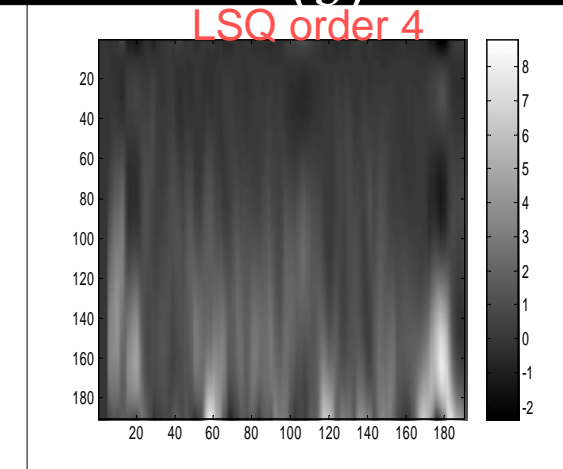
(b)

LSQ order 3



(c)

LSQ order 4



(d)

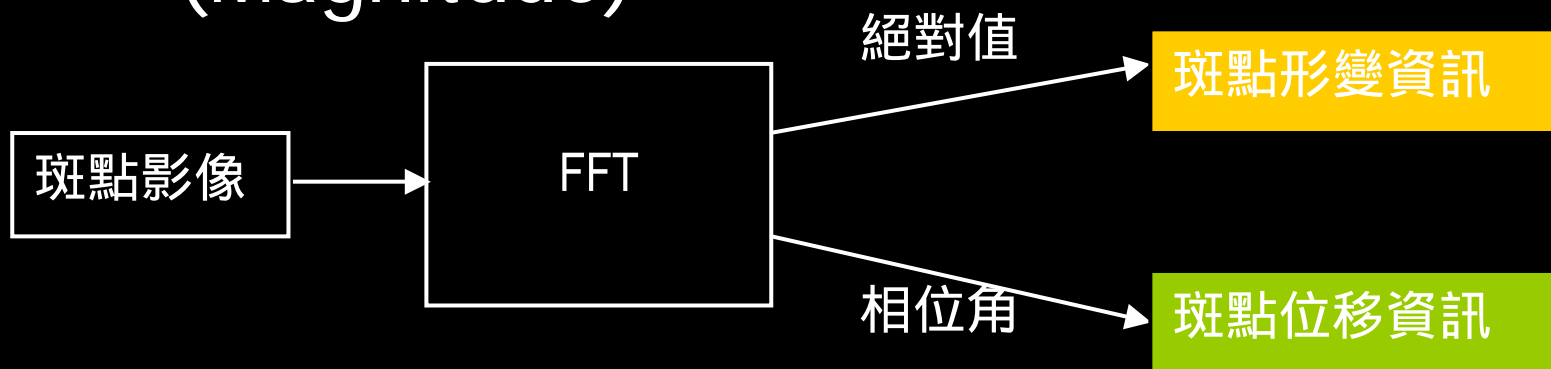
# FFT-based Speckle Analysis

---

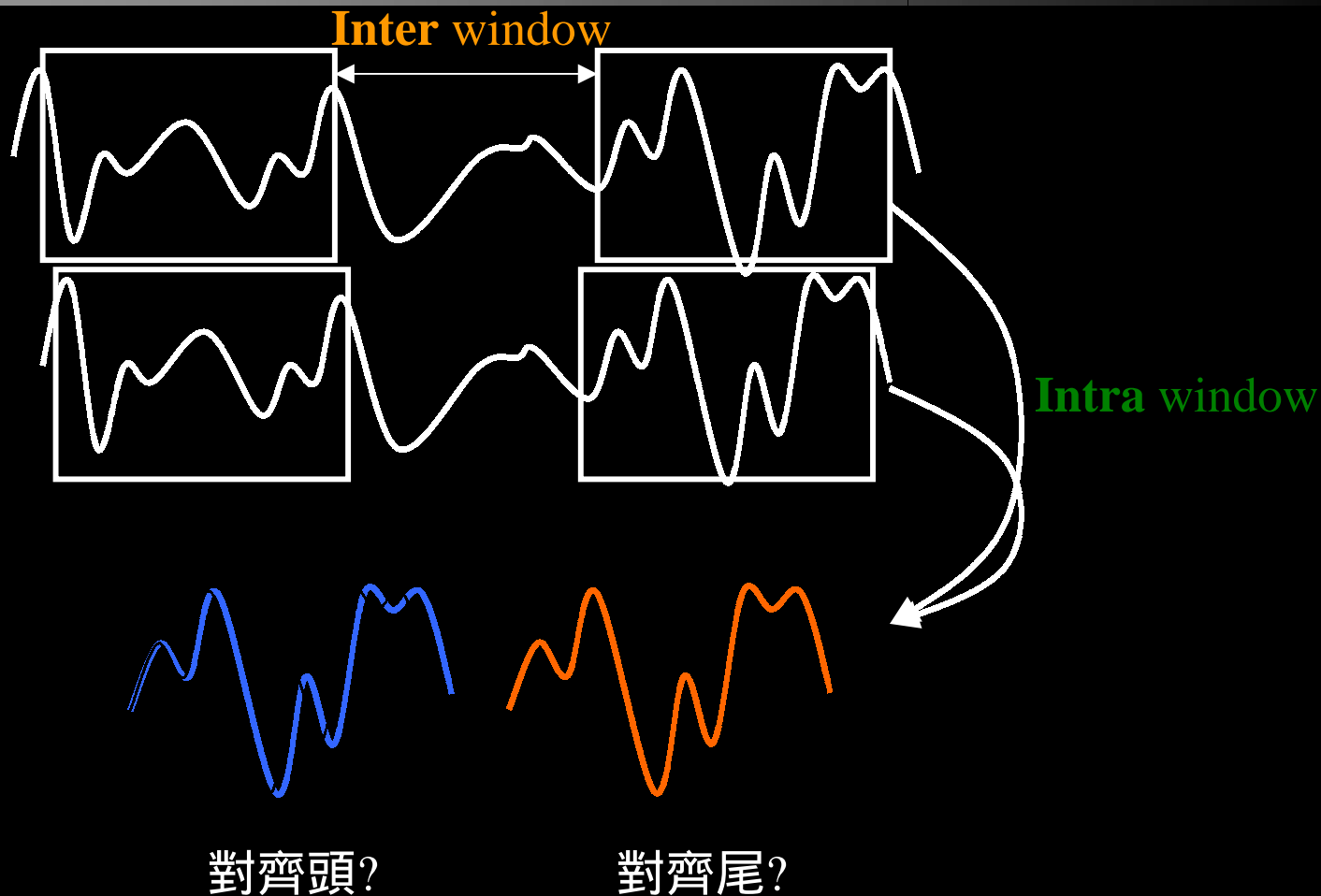
- 報告內容：
  - 原理說明—FFT之特性及優點
  - 文獻參考—Temporal Stretch Method
  - 方法與步驟
  - 結果與討論

# 原理說明—FFT之特性及優點

- FFT為快速演算法
- 具有 translation invariant特性 (Magnitude)

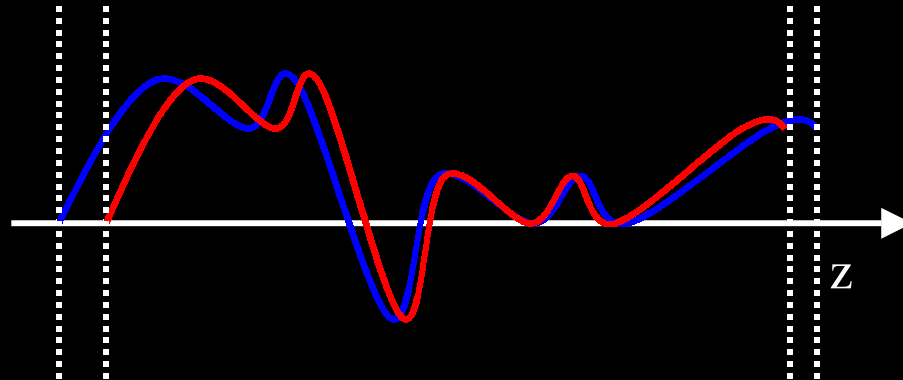


# 文獻參考—Temporal Stretch



# FFT-based Speckle Analysis

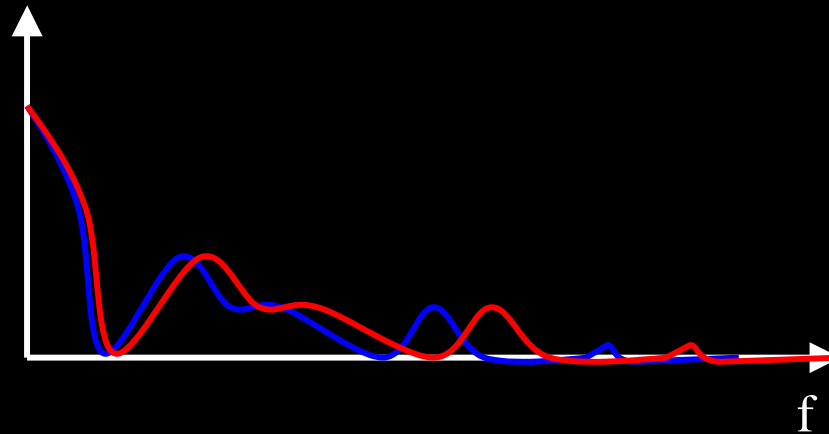
- 由頻域對B-mode影像進行分析
  - Z軸方向的一段組織反射信號



# FFT-based Speckle Analysis

- 信號與系統理論：

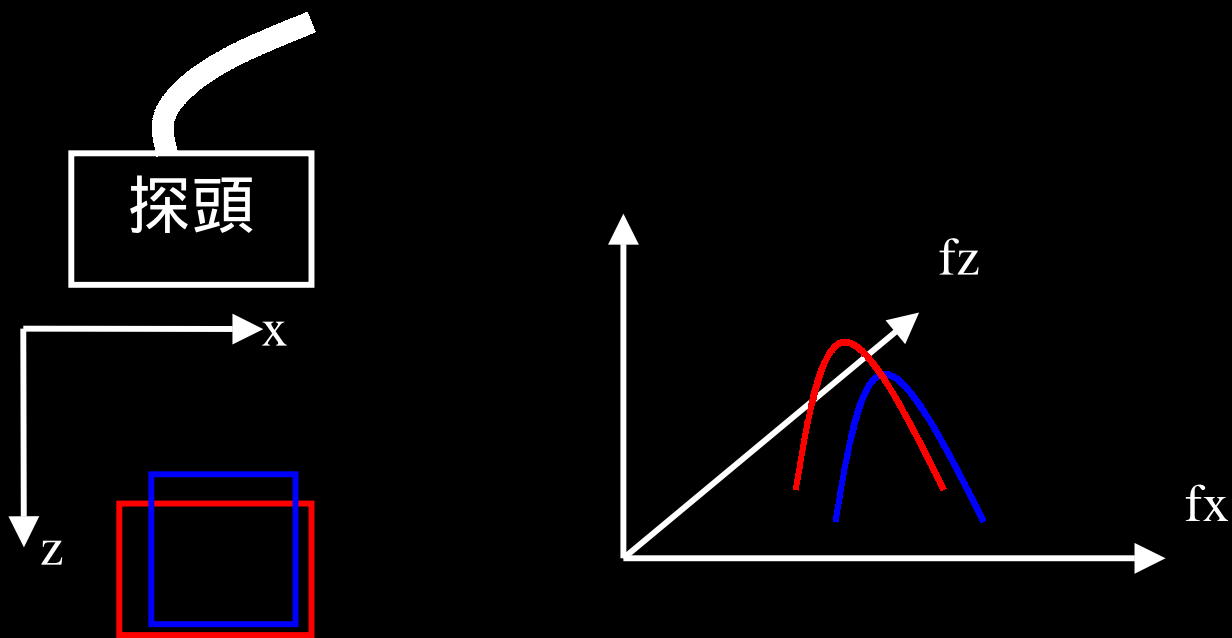
- $a(z) \rightarrow A(\quad)$
  - $a(kz) \rightarrow A(\quad/k)$





# FFT-based Speckle Analysis

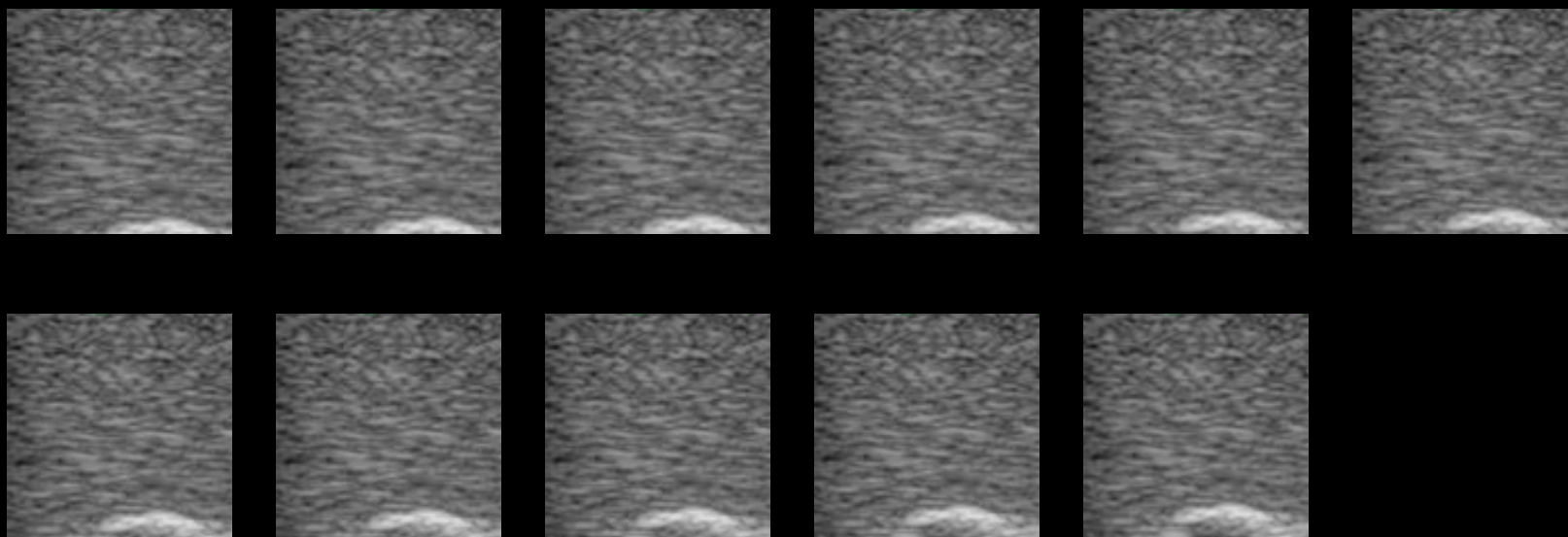
- 將此方法推廣至二維：



# 方法步驟—形變分析

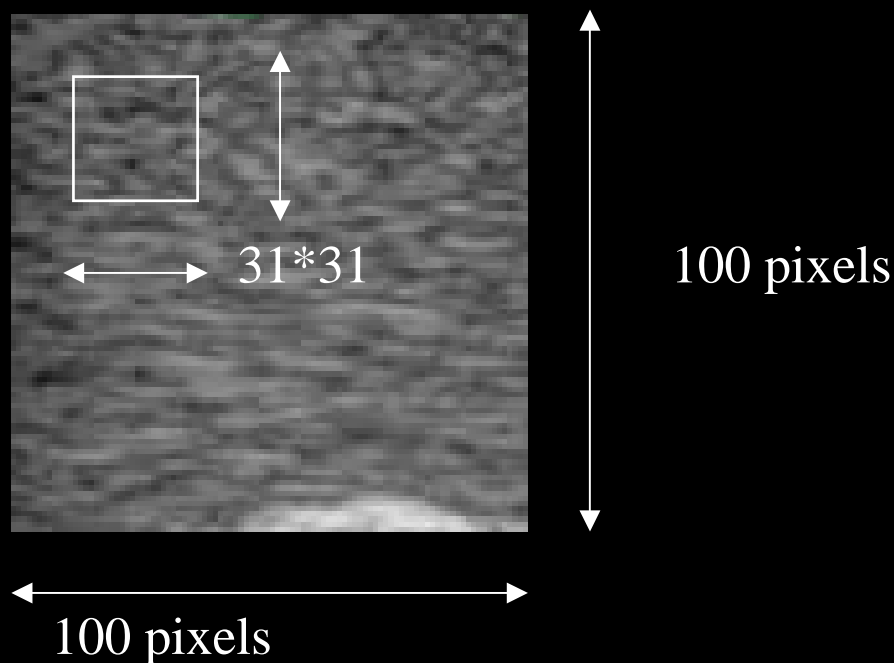
---

- 使用一系列以photoshop進行縮放調整之speckle影像進行模擬



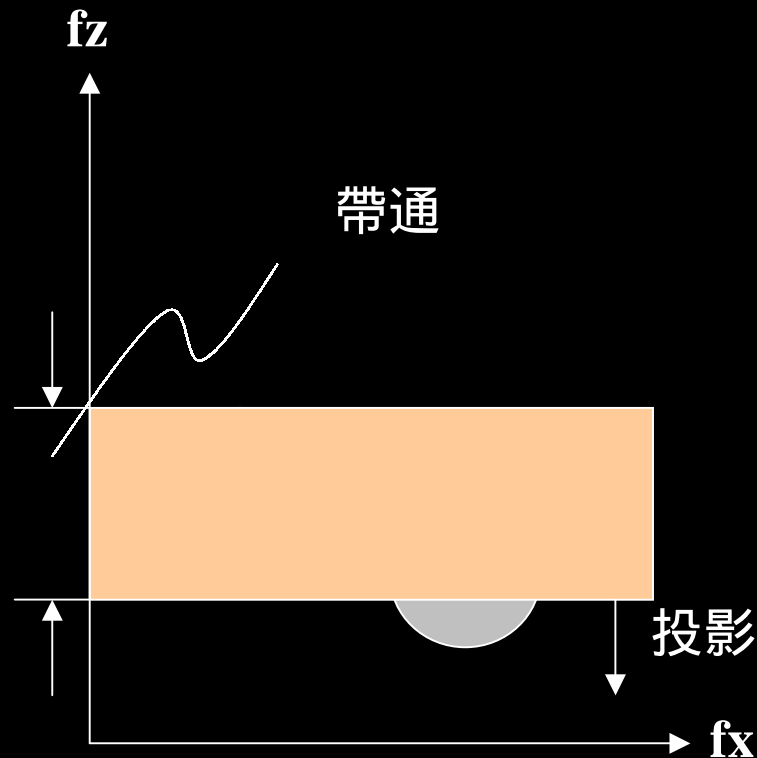
# 方法步驟—形變分析

- 將每張影像取出 $31 \times 31$  pixels部分進行分析(不包含亮點)

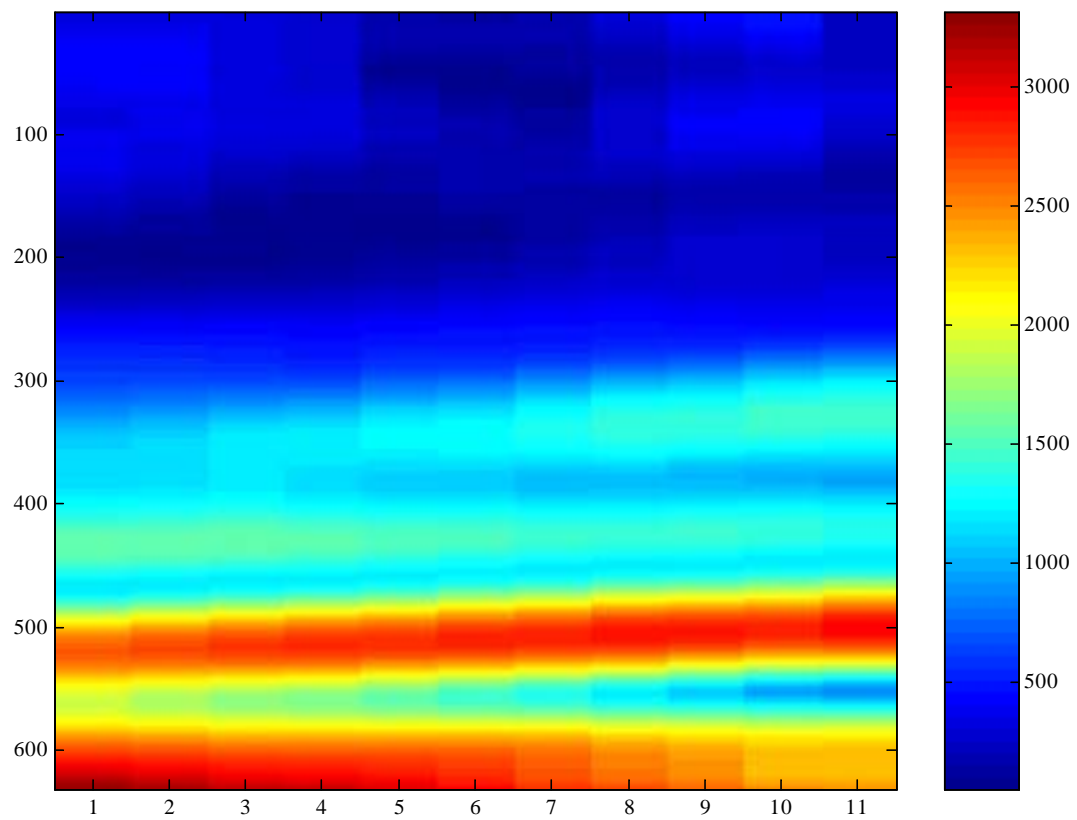


# 方法步驟—形變分析

- 富利葉轉換後，保留正頻率之magnitude用來分析相鄰frame間，是否有頻率shift

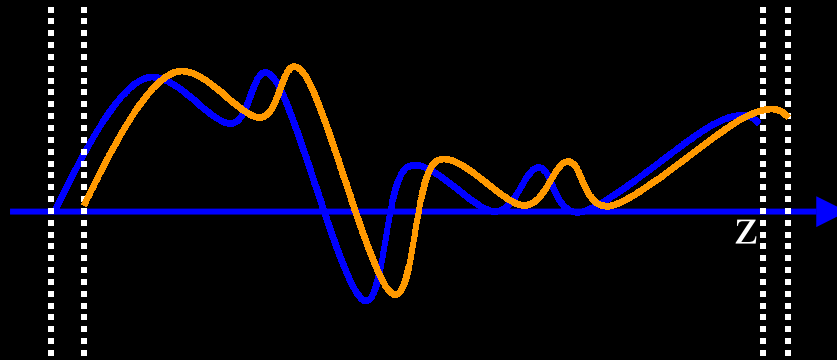


Spectrum

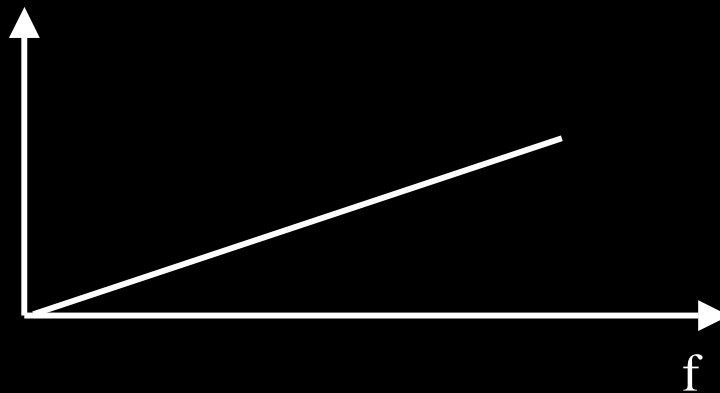


Frame

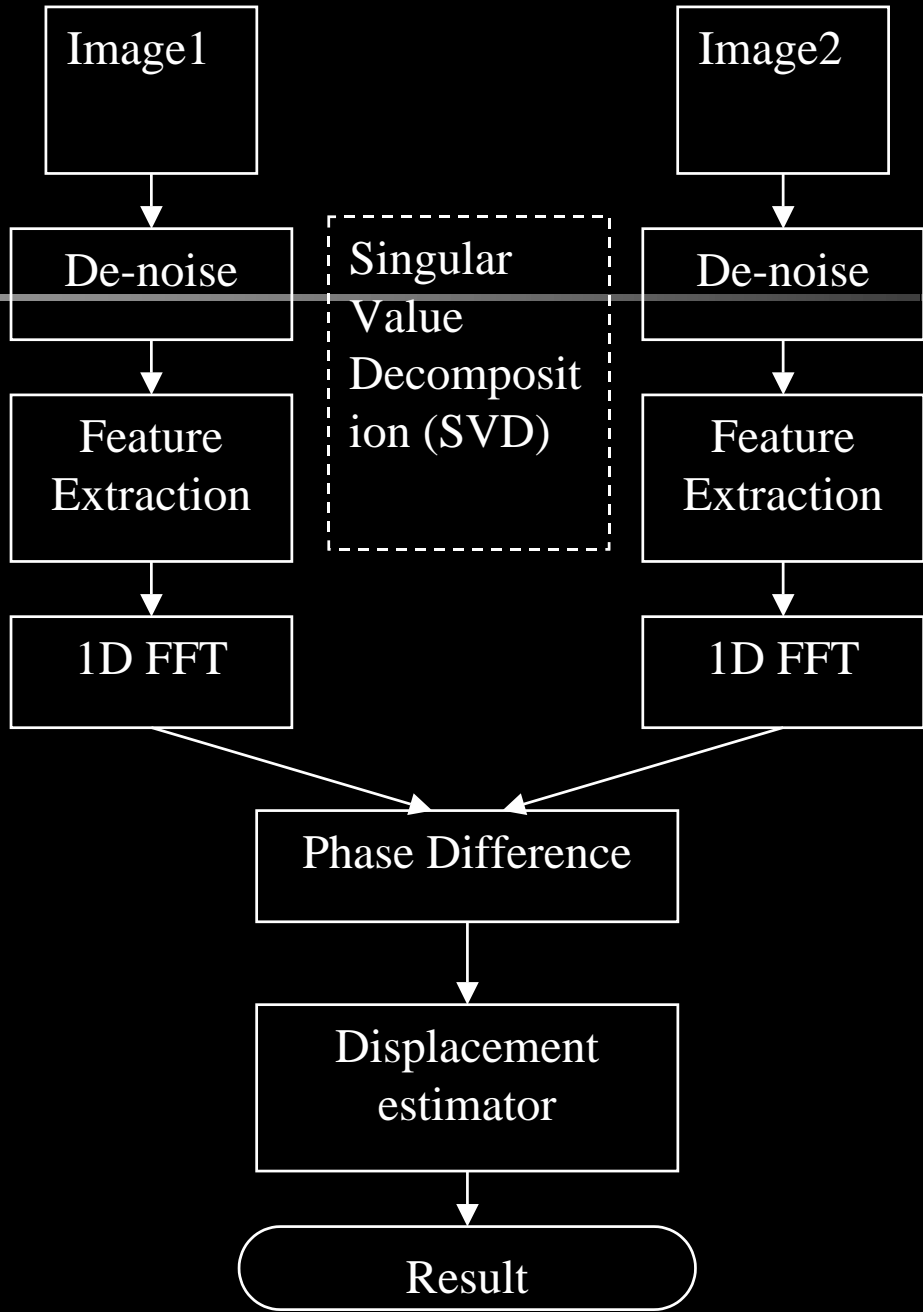
# 方法步驟—位移分析



Phase difference



$$\phi = 2\pi * z$$



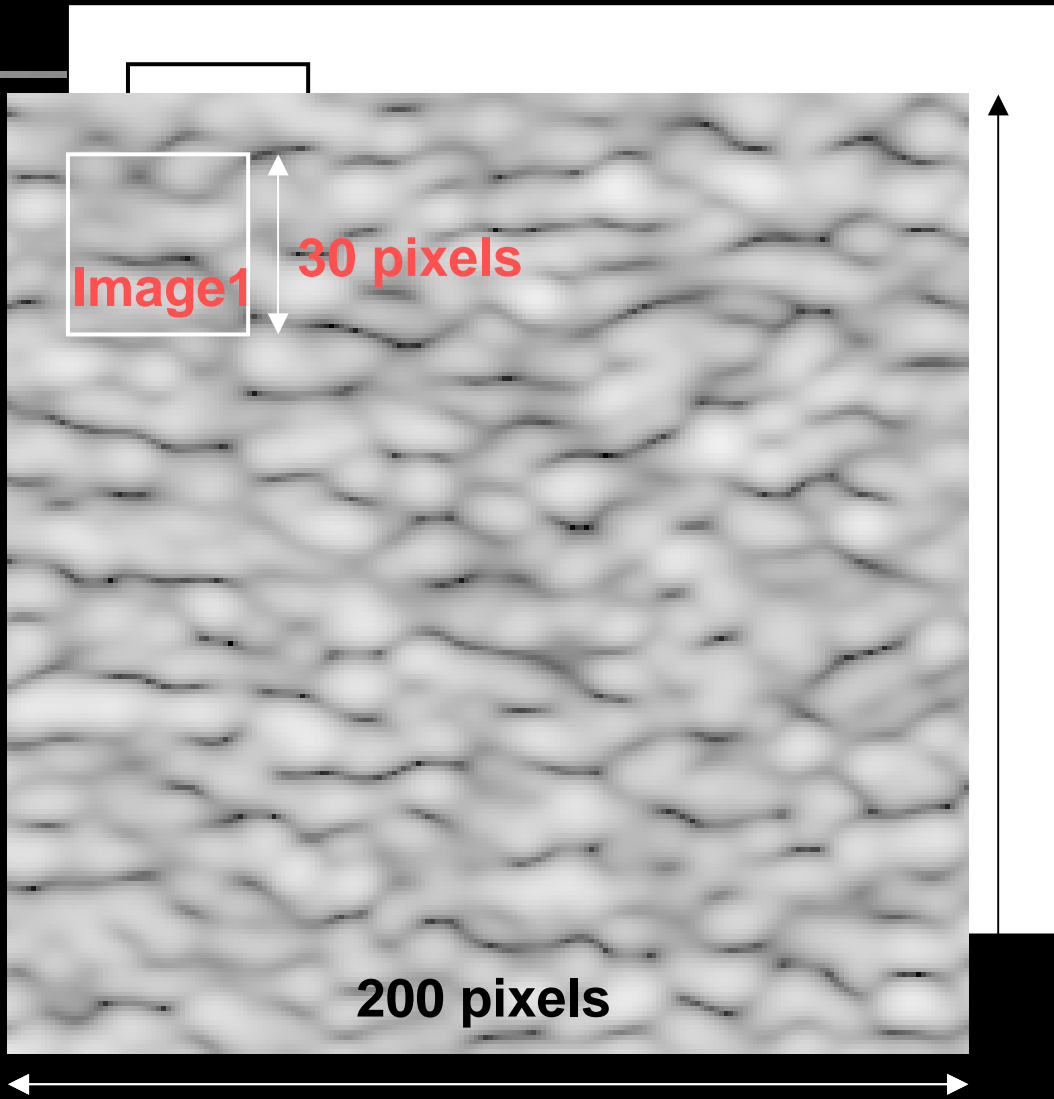


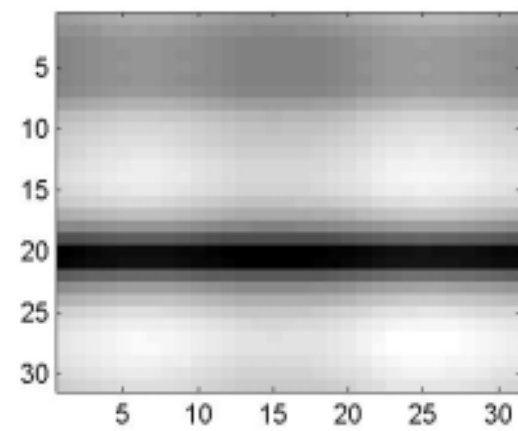
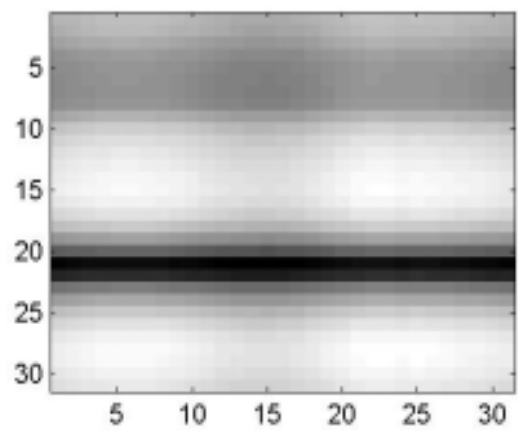
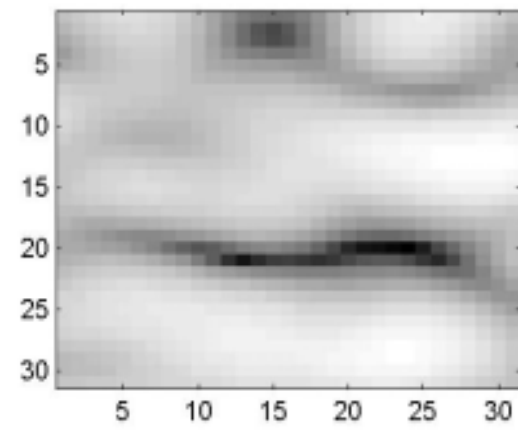
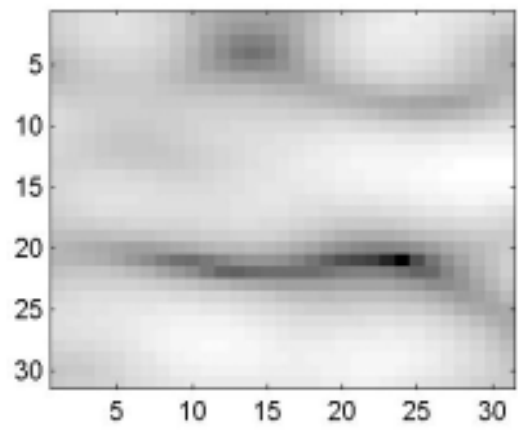
Image1

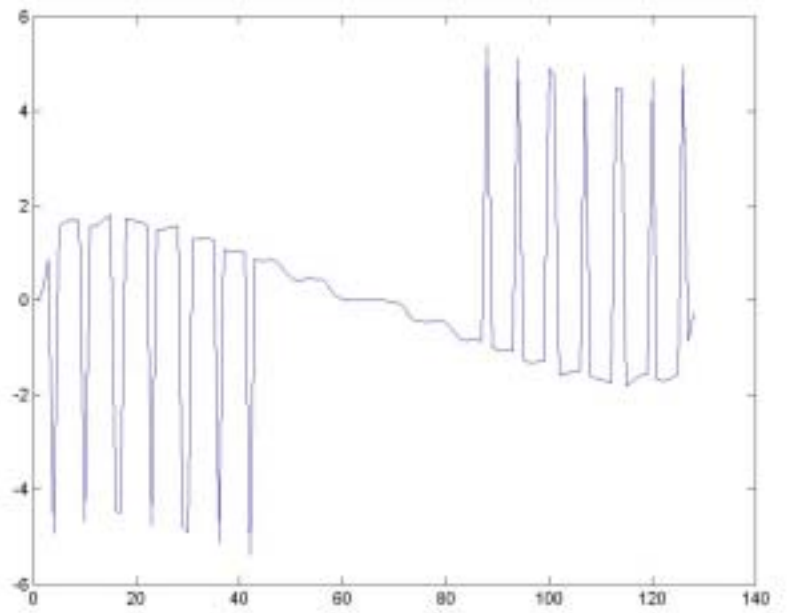
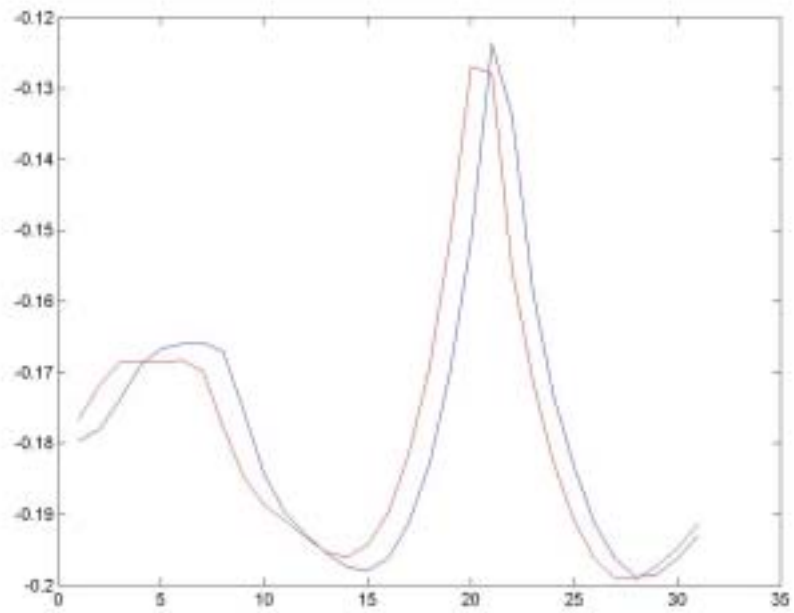
30 pixels

200 pixels

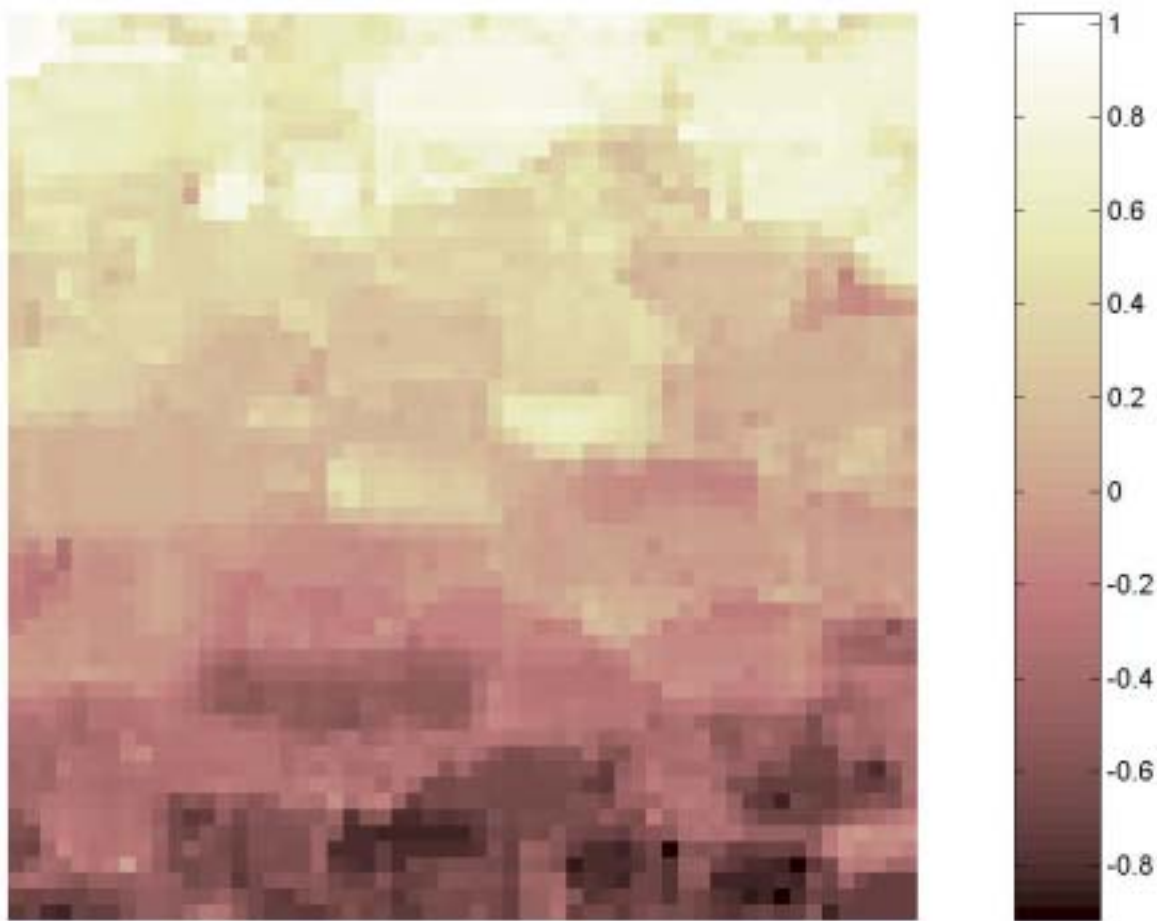


**SVD**  
**1'st eigen**  
**image**





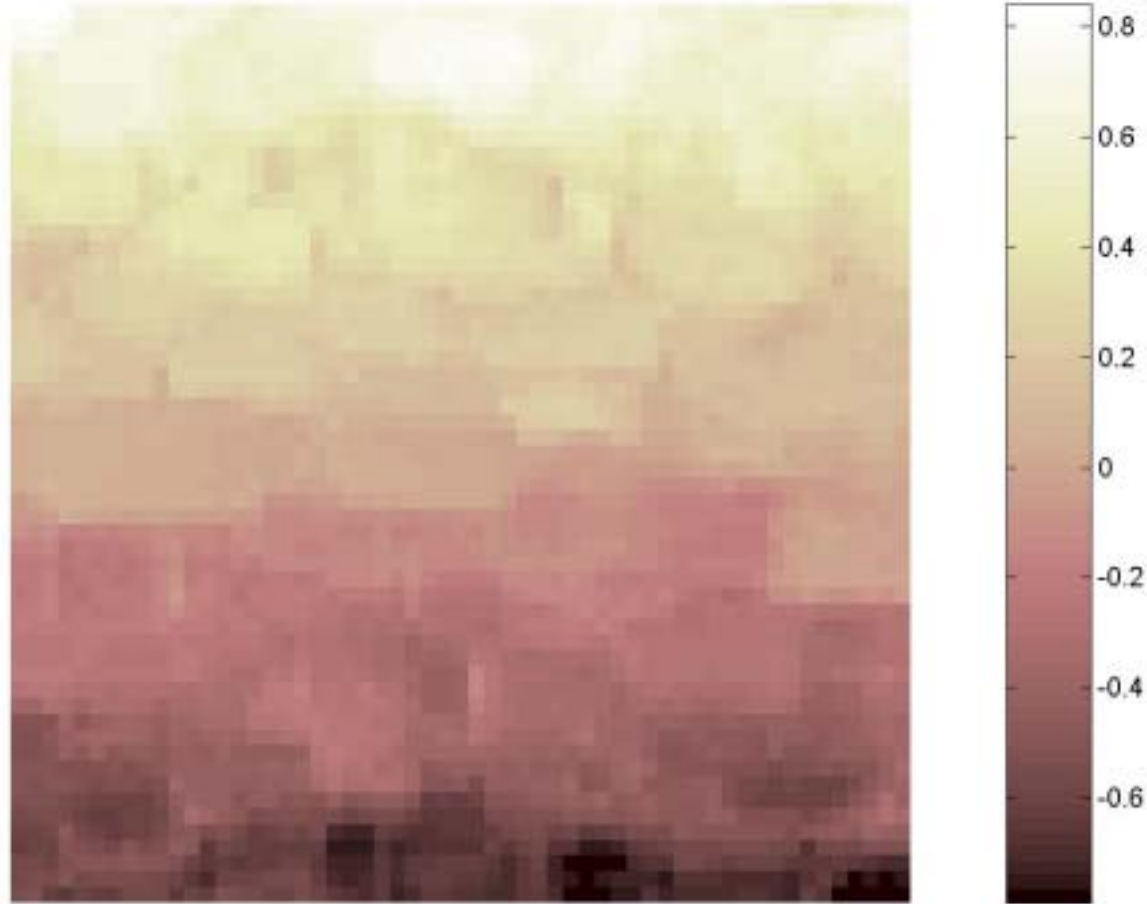
Z axis displacement image



↓  
位移量  
向下為正  
單位 pixel

以兩張相鄰strain $\sim$ 1%之影像計算所得結果。

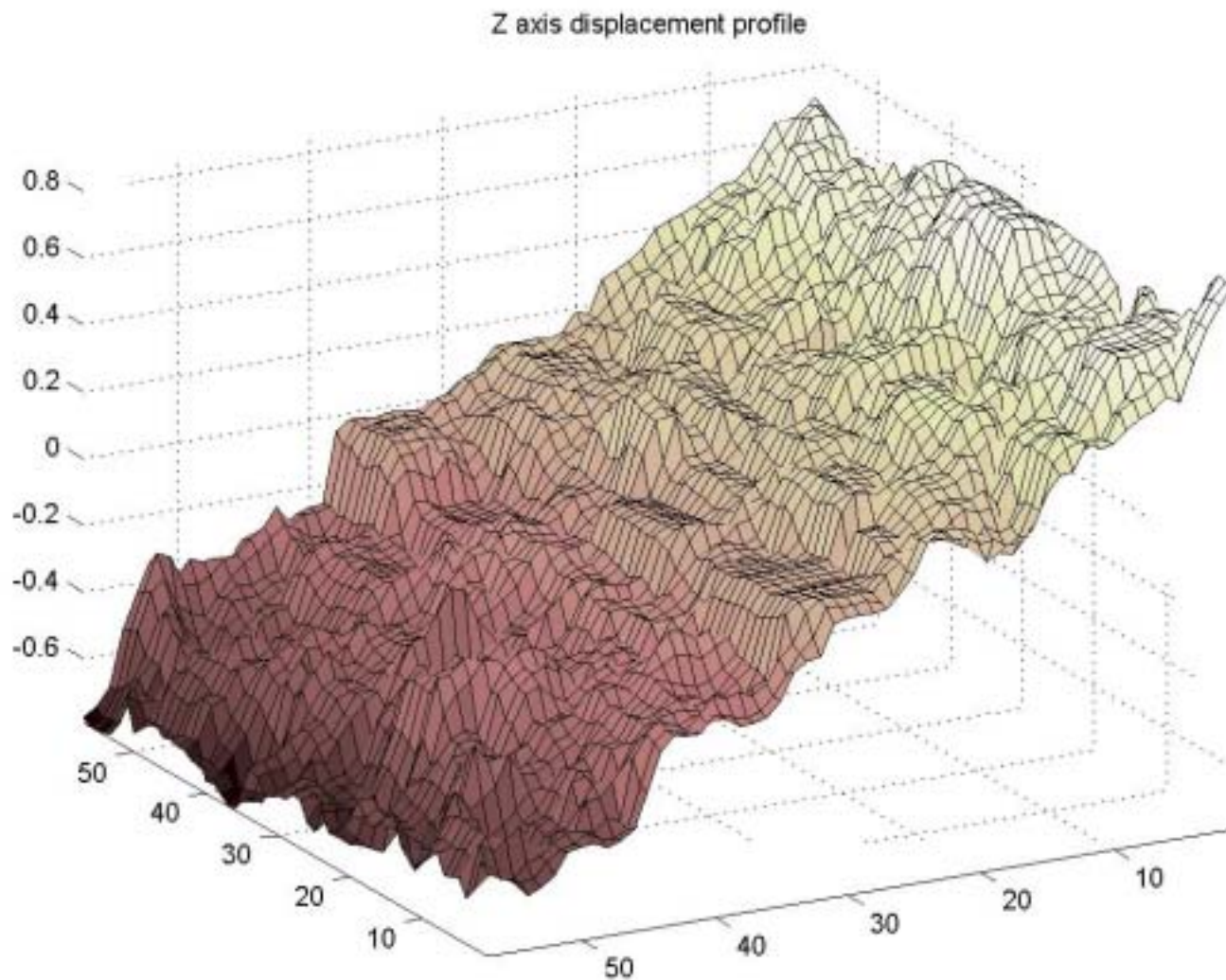
Z axis displacement image



↓  
位移量  
向下為正  
單位 pixel

以十一張相鄰strain $\approx$ 1%之影像計算所得結果。  
(十張displacement影像複合之結果)

↓  
位移量  
向下為正  
單位 pixel



同上一結果（十一張相鄰像計算所得）。  
以profile表示，可以看出其線性程度。

# 討論

---

- 壓縮1%的200\*200模擬影像，確實可以偵測出  $\pm 1$  pixel 漸層變化的位移量。
- spatial domain的filter、constrain都尚未派上用場。
- strain是位移量的微分。
- 如果有簡便之類似運算可代替SVD，將比傳統speckle tracking大幅節省運算量。

# Discussion

---

- 1D method has higher sensitivity, but also higher noise (lower correlation coefficients).
- More diffuse distribution of strain signal than 2D method
- 2D method has higher precision rate (high correlation coefficients) and best  $X$  direction displacement estimate.
- Band like strain signals were estimated for simulation and phantom images, the cause may be due to quantitative error (accumulated of tiny strain relieved at the similar row)

# Discussion

---

- For clinical breast tumor images, 1D and 2D method could detect the strain both.
- Multiple level speckle tracking method would produce obvious error and is not suitable for ultrasonic strain estimation.
- Full search sum of difference method has near similar high precision rate as the correlation coefficients method
- Interpolation could increase the sensitivity but also the noise, long time period was used in calculation.



# Future work

---

- Try the least square strain estimator proposed by Ophir group for smoothing the images(denoise?) in 1D (1 method?)
- Applying pyramid method for fasting the calculating speed of sum of difference method.
- Improving the interpolation method for reducing the noise.

# References

---

- Yong-Sheng Chen, Yi-Ping Hung, Chiou-Shann Fuh "Fast Block Matching Algorithm Based on the Winner-Update Strategy" IEEE Trans on Image Processing 2001 ; 10 (8): 1212-1222.
- Yeung F, Levinson SF, Parker KJ. Multiplevel and motion model-based ultrasonic Speckle tracking algorithms. Ultrasound in Med. & Biol 1998; 24(3): 427-441.
- Gao L, Parker KJ, Lerner RM, Levinson SF. Imaging of the elastic properties of tissue-a review. Ultrasound in Med. & Biol 1996; 22(8): 959-977.
- Ophir J, Cespedes I, Ponnekanti H, yazdi Y, Li X. Elastography: a quantitative method for imaging the elasticity of biological tissues. Ultrasonic imaging 1991; 13;111-134.
- O'Donnell M, Skovoroda AR, Shapo BM, Emelianov SY. Internal displacement and strain imaging using ultrasonic speckle tracking. IEEE Trans. Ultrason. . Ferroelect Freq. Contr. 1994;41(3):314-325.
- Konofagou EE, Harrigan T, Solomon S. Assessment of regional myocardial strain using cardiac elastography: distinguishing infarcted from non-farcted myocardium. 2001 IEEE ultrasonics symposium: 1589-92.